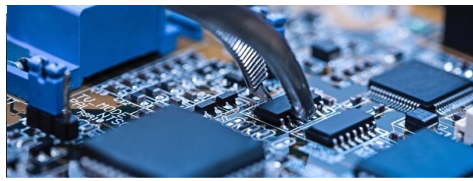
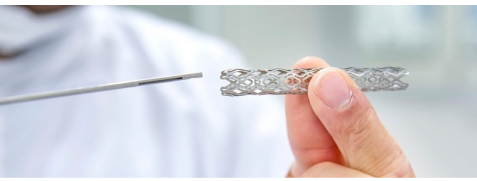
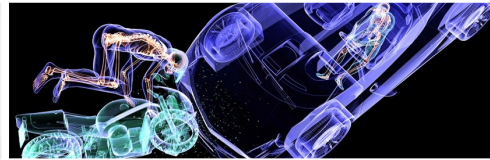


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Medical Device Design and Infection Prevention: What Do Manufacturers Need to Know?

**Medmarc Insurance Group
Webinar Series**

June 15, 2021

Howard Loree, Ph.D.



- Background
 - Presenter
 - Exponent
- Medical Device Infections
 - Costs
 - Causes
- Design Strategies for Infection Prevention
 - Single Use Devices
 - Reusable Devices
- Device Use and Environment
- Design Verification & Validation for Infection Prevention
- Conclusions
- Q & A

Background

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Education

- Ph.D. Medical Engineering
Harvard – MIT HST
- M.S. Mechanical Engineering
MIT
- B.S. Mechanical Engineering
MIT

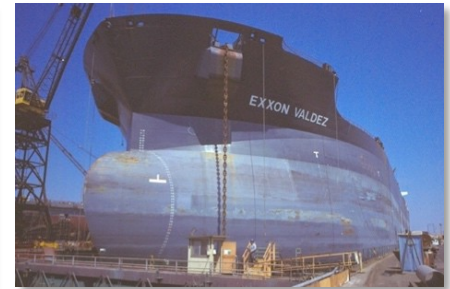
Experience

- Complete product development life cycle for medical devices, especially cardiovascular
- Expert in mechanical circulatory support
- Technology assessment, product design optimization, and NIH grant strategy

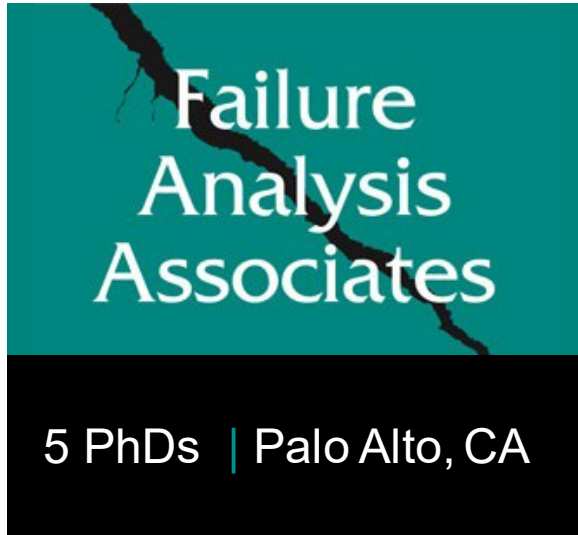
Positions

- Exponent, Manager (2020-Present)
- Flow Forward Medical, VP of R&D (2011-2020)
- Metactive Medical, VP of R&D (2013-2018)
- Avedro, VP of Research & Chief Scientist (2009-2010)
- ABIOMED, Principal Staff Scientist (2006-2009)
- Orthopeutics, VP (2005-2006)
- Thoratec, Manager of Research (2002-2005)
- Thermo Cardiosystems / Thoratec, Senior Scientist (1995-2002)
- Brigham and Women's Hospital, Harvard Medical School, Postdoctoral Research Fellow, Cardiovascular Biomechanics (1992-1995)

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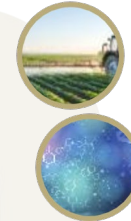
Mechanical & Thermal

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- Mechanical Engineering



Health Sciences

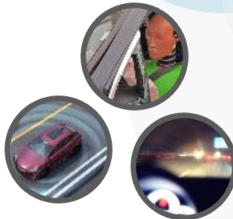
- Chemical Regulation & Food Safety
- Health Sciences



PROJECTS

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- Human Factors
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- Civil Engineering
- Construction Consulting
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- Statistical & Data Sciences



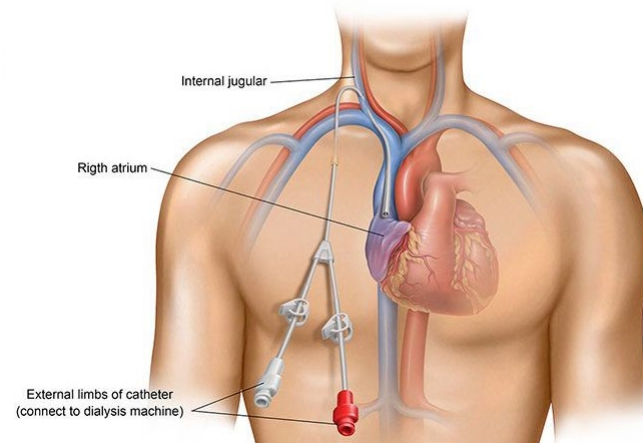
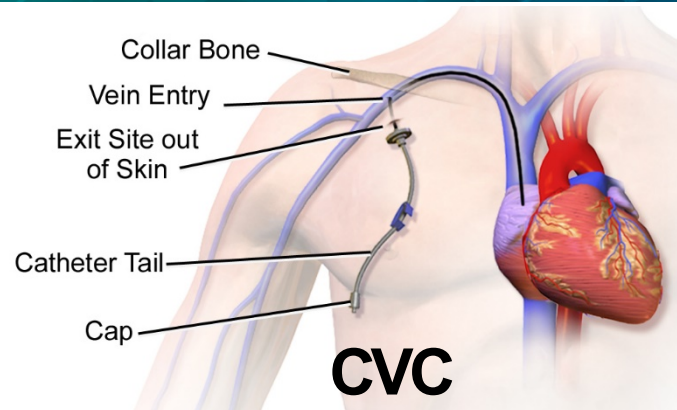
Medical Device Infections

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- Healthcare-associated infections (HAIs)
 - The overall annual direct medical costs of HAIs to US hospitals range from \$37B to \$58B.¹
 - The benefits of prevention range from \$32B to \$41B, assuming that 70% of infections are preventable.¹
- **Medical device infections**
 - Of the nearly 2 million HAIs reported by CDC, 50–70% can be attributed to indwelling medical devices.²⁻⁴
 - **Based on the above estimates, costs range \$18B to \$29B, of which \$16B to \$20B could be saved through prevention.**
 - Attributable mortality is highly device dependent but can range from < 5% for devices such as dental implants and foley catheters to > 25% for mechanical heart valves.⁴

Catheter Infections

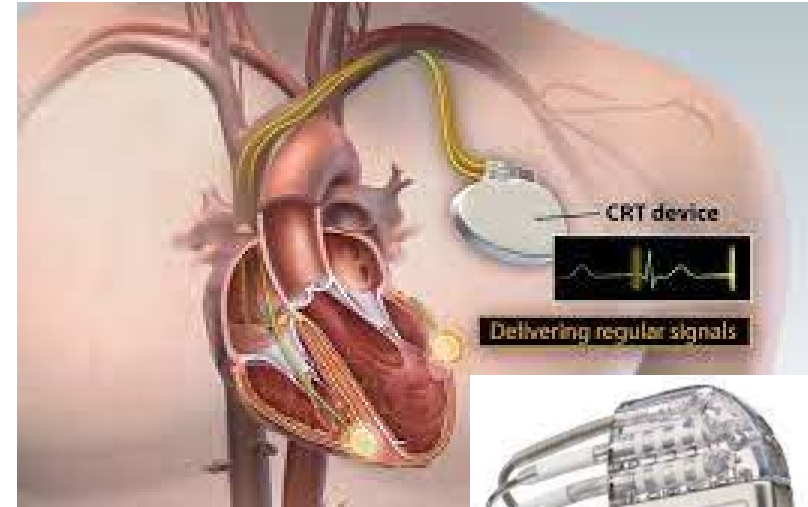
- There are over 15M patient days of exposure to central venous catheters (CVCs) in US ICUs annually.⁵
 - Incidence of non-dialysis catheter related bloodstream infection ranges 2.5 - 4 per 1000 catheter days.^{6,7}
- Hemodialysis (HD) catheters have higher infection rates.
 - These range 3.8 - 5.5 per 1000 catheter days.^{7,8}
 - In the ICU these infections can equate to financial costs as high as \$30K per infection with the potential for increased duration of mechanical ventilation, 1 wk increased ICU stay, and 2–3 wks of additional hospital stay.^{9,10}



HD Catheter

Cardiac Device Infections

- Cardiac implantable electronic devices (CIEDs) include pacemakers (IPGs), implantable cardioverter-defibrillators (ICDs), and cardiac resynchronization therapy (CRT) devices.
- The incidence of cardiac device infections (CDIs) averages 1.2 - 1.6%,¹¹ but can be > 4% for high-risk patients.¹²

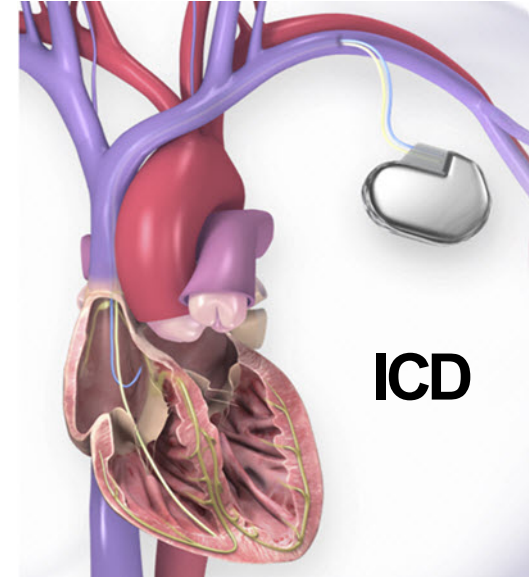


CRT Device



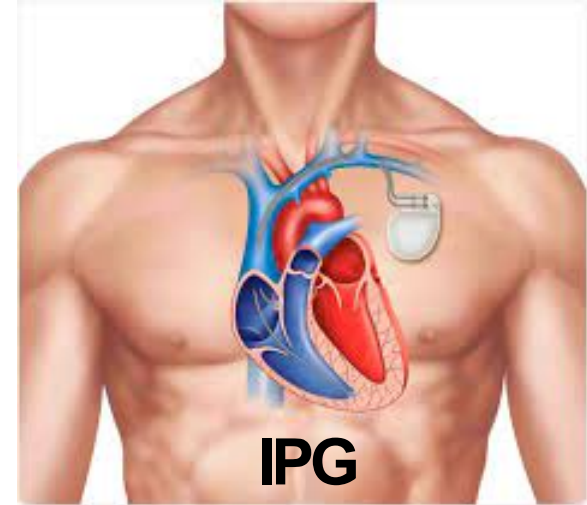
Cardiac Device Infections (Cont.)

- CDI rates have not only increased over time, but several studies suggest the increase in CDI rate has outpaced the increase in device implantation rate.¹³⁻¹⁵
- CDIs are associated with substantial morbidity, mortality, prolonged hospital length of stay (LOS), as well as procedures for device & lead extraction and subsequent reimplantation.^{13,16-19}



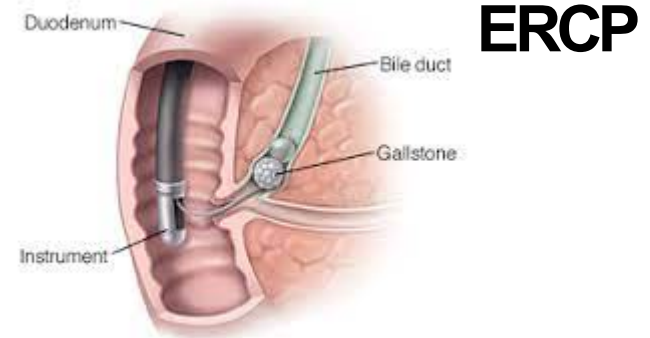
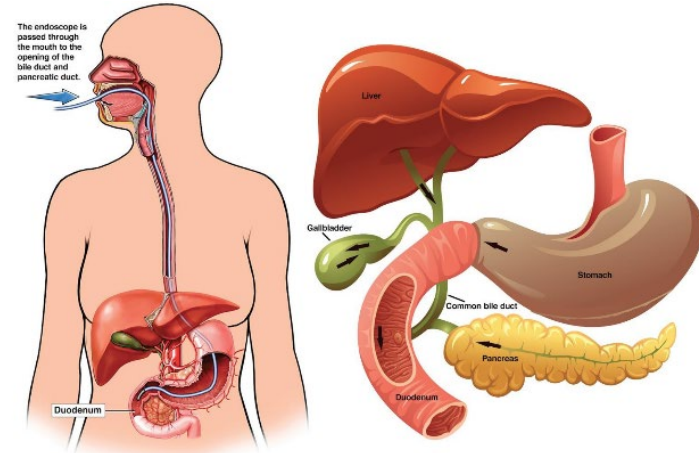
Cardiac Device Infections (Cont.)

- CDIs are extremely costly to the healthcare system, with hospital charges ranging from \$125K to \$250K for inpatient admissions with a CDI-related extraction.¹⁵
- The total mortality in the case of CDIs is estimated at 9 - 35% during the first year after implantation.^{17,21-24}



Endoscope Infections

- Over 500,000 endoscopic retrograde cholangiopancreatographies (ERCP) are performed annually in the US.²⁵
- Contaminated endoscopes cause more healthcare-associated infection outbreaks than any other medical device.^{26,27}
- While some outbreaks have been associated with inadequate reprocessing of endoscopes, epidemics have occurred even without lapses in decontamination procedures.²⁸⁻³⁶



Endoscope Infections (Cont.)

- The duodenoscope is among the most complex medical instruments that undergo disinfection between patients.
- Transmission of infection by device contamination has remained a challenge since its inception.
- Risk factors include non-adherence to disinfection guidelines, biofilm deposition due to complex design and surface defects, and contaminated automated endoscope reprocessors (AERs).³⁷



Duodenoscope



Endoscope Infections (Cont.)

- From January 2010 to October 2015, more than 400 patients were infected at US hospitals during ERCP procedures.
- The infections often included antibiotic-resistant bacteria. The most notable was carbapenem-resistant Enterobacteriaceae (CRE), associated with a 50% mortality rate.
- Lawsuits were filed against duodenoscope manufacturers. A jury handed up an initial award of \$6.6M in 2017.³⁸
- In 2018, FDA issued warning letters to all 3 manufacturers for failure to provide sufficient data to address postmarket surveillance studies.³⁹



Root Causes of Medical Device Infection

- Organisms originate from colonizing microbiota of patients or healthcare workers, or environmental sources.
- Antimicrobial resistance is expanding and evolving.
- Ineffective sterilization or poor sterile technique during implantation leads to device contamination.
- Inadequate cleaning of reusable instruments causes cross-contamination between patients.
- Poor aseptic technique in wound / exit site care allows pathogens to enter device, tunnel, or pocket.
- Bacteria form biofilms, which inhibit action of antibiotics and patient's immune system.

Design Strategies for Infection Prevention

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Example: Medtronic TYRX Envelope

- Large-pore mesh knitted from bioabsorbable filaments
- Coated with bioabsorbable polyarylate polymer formulated with antibiotics (*i.e.*, minocycline & rifampin)
- Elutes locally into tissue pocket
- Fully absorbs into body within ~ 9 wks⁴⁰



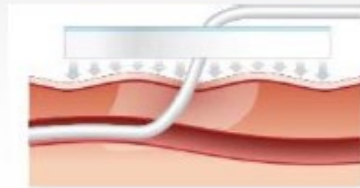
WRAP-IT Trial⁴¹

Number of Participants (n)	Study Population	Study Design	Follow-up Duration	Results
6,983	High-risk CIED implantation (<i>e.g.</i> , replacement, upgrade, revision, or CRT procedures)	Antibiotic-impregnated mesh envelope vs. control	12 mos	Decreased CIED infection rate with envelope (0.7%) vs. control (1.2%) ($p = 0.04$)

Example: Ethicon BIOPATCH

- Urethane disc adhered to skin around percutaneous devices (e.g., catheters)
- Elutes chlorhexidine gluconate (CHG) over 7 days to maintain skin antiseptics⁴²

60% reduction in catheter-related bloodstream infections as compared with standard care (P=.026)¹



44% reduction in local infections as compared with standard care (P≤.0001)¹

43

Use with both vascular and nonvascular percutaneous devices



Central Venous Catheters



Dialysis Catheters



Arterial Catheters



PICC Lines



Peripheral IVs



Mid Lines



Epidural Catheters



Implanted Venous Ports



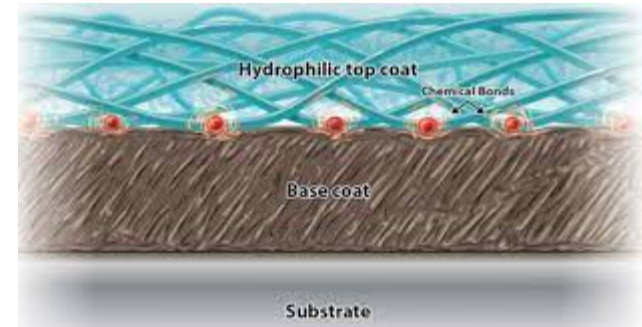
External Fixator Pins



Drains

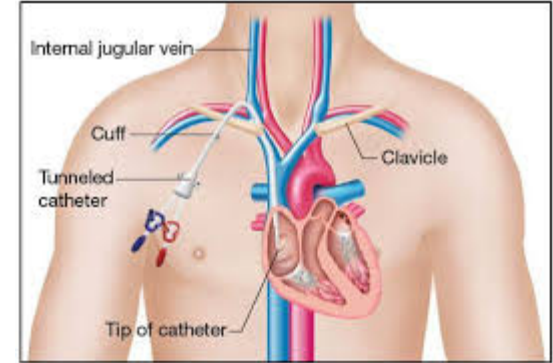
Example: Surmodics Serene™ Coating

- Covalently bonded, UV cured
- Compatible with Pebax®, nylon, PEEK, HDPE, and a wide variety of other substrates
- Extremely thin coating with low friction and low particulates
- Reduces bacterial adherence
- Can be formulated with antimicrobial and antithrombotic agents⁴⁴
- Similar coatings shown to reduce infection rate by 50% for urologic implants^{45,46}
- Widely used but not yet shown efficacy for urinary catheters⁴⁷



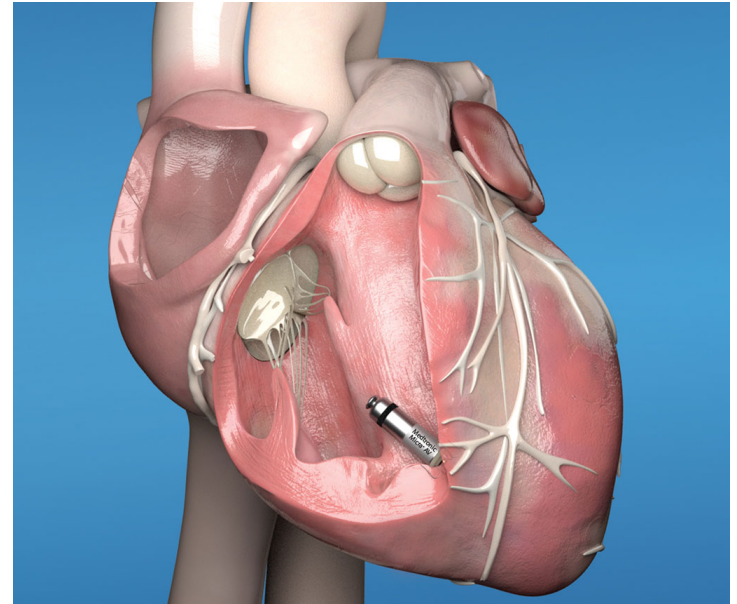
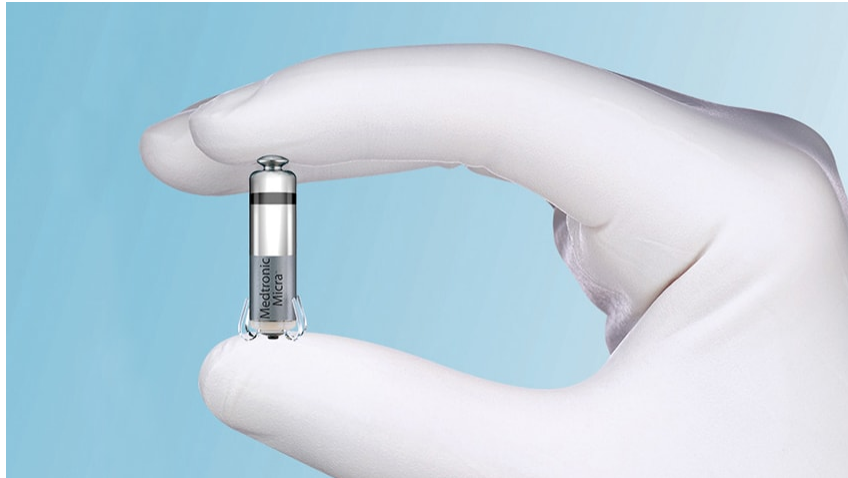
Example: Cuffed Tunneled HD Catheter

- Tunneled HD catheters are associated with lower rates of infectious complications compared with non-tunneled catheters.
- The catheter is generally placed so that the polyester felt cuff is positioned subcutaneously 1 - 2 cm from the skin exit site.
- Tissue ingrowth into the cuff seals off the catheter tunnel to reduce the risk of infection.
- Tunneled HD catheters are primarily used for intermediate or long-term vascular access.



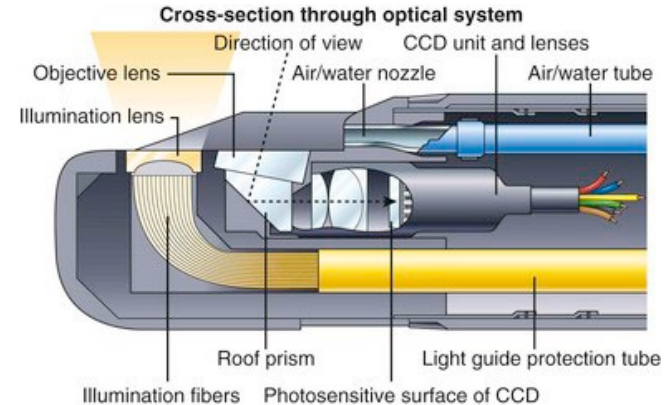
Example: Medtronic Micra

- 90% smaller than a transvenous pacemaker, placed directly into right ventricle
- Eliminates several complications associated with transvenous pacemakers and leads: pocket infections, hematoma, lead dislodgment, and lead fracture
- Currently limited to right ventricular pacing
- No long-term outcome data yet available^{47,48}



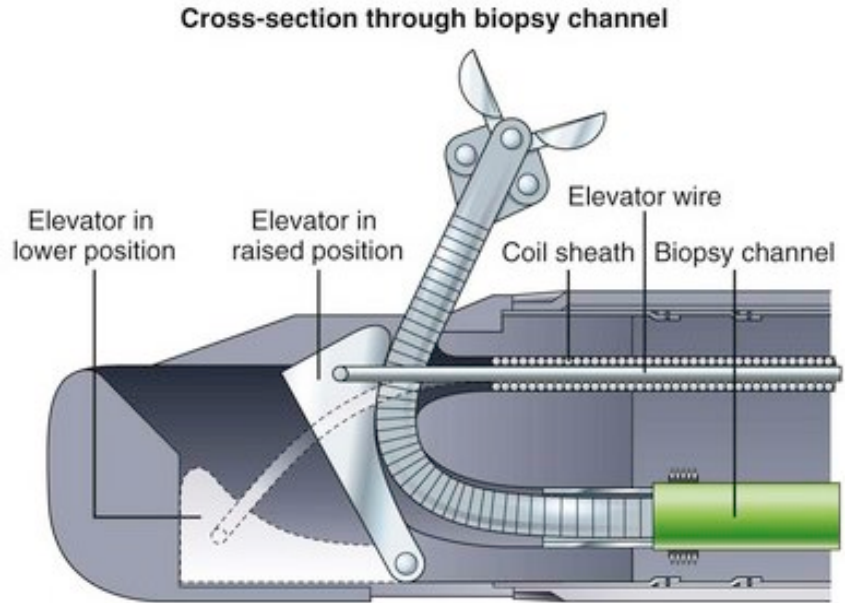
Reusable Endoscope Design Guidelines

- FDA's evaluation of adverse event reports and other information identified design features that are prone to retaining debris and biological materials, including:⁵⁰
 - Long, narrow interior channels (lumens), including those with internal surfaces that are not smooth, have ridges or sharp angles, or are too small to accept a brush
 - Hinges
 - Sleeves surrounding rods, blades, activators, inserters, etc.
 - Adjacent device surfaces between which debris can be forced or caught during use
 - O-rings
 - Valves that regulate the flow of fluid through a device (stopcocks)
 - Devices with these or other features that cannot be disassembled for reprocessing



Reusable Endoscope Design Guidelines (Cont.) ^{Ex}

- From the earliest stages of device design and engineering, manufacturers should consider alternative designs to facilitate effective reprocessing:⁵¹
 - Replace features that are challenging to reprocess with single-use parts
 - Include flush ports
 - Specify and/or provide dedicated cleaning accessories



Single Use Endoscope

Example: Ambu aScope Duodeno



- Packaged sterile
- No reprocessing / repair
- Familiar design⁵²



Gas: Low temperature, but require permeable packaging & product design

- Ethylene oxide
 - Penetrates multiple layers of packaging and hard-to-reach places (*e.g.*, catheters)
 - Compatible with most materials
 - Cycle time: Days
 - Environmental hazard, so providers face increasing regulatory challenges
- Hydrogen peroxide
 - Limited penetration relative to ethylene oxide
 - Only residuals are water and oxygen
 - Cycle time: Hours
 - Devices must be free of moisture

Radiation & Heat: Limited material compatibility

- Gamma or X-rays
 - Precise control of dose and penetration
 - No chemical residuals
 - Cycle time: Hours
 - Incompatible with acetals, PTFE, or unstable polypropylene; causes color changes in some polymers (e.g., PVC and polycarbonate) unless stabilized with additives
- Steam or dry heat
 - Low processing and capital cost, often done in-house
 - Cycle time: Minutes to hours
 - Suitable for glass and metal (e.g., pharmaceutical vials and surgical tools)
 - Incompatible with electronics or complex assemblies

Device Use and Environment

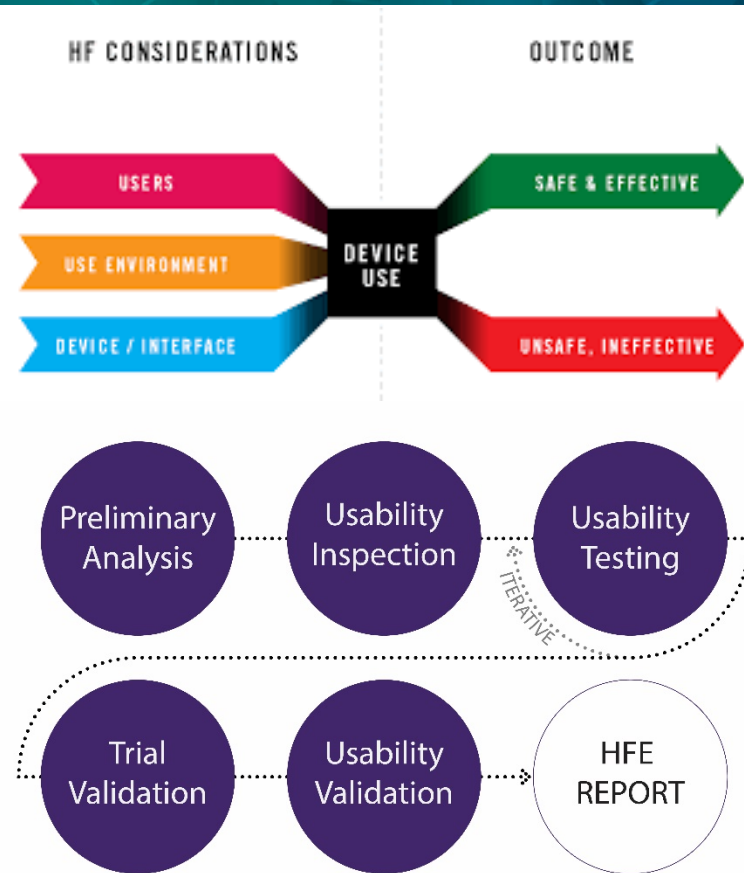
Ex

THE NATURE OF ADVERSE EVENTS IN HOSPITALIZED PATIENTS

Results of the Harvard Medical Practice Study II⁵³

- The most extensive study of adverse events: more than 30,000 randomly selected discharges from 51 randomly selected hospitals in NY in 1984.
- Adverse events, manifest by prolonged hospitalization or disability at the time of discharge or both, occurred in 3.7% of the hospitalizations.
- The **proportion of adverse events attributable to errors (i.e., preventable adverse events) was 58%** and to negligence was 27.6%.
- Although most of these adverse events gave rise to disability lasting < 6 mos, 13.6% resulted in death and 2.6% caused permanently disabling injuries.
- Drug complications were the most common type of adverse event (19%), followed by **wound infections (14%)** and technical complications (13%)

- Use errors can often be attributed to the design of devices or processes.
- For medical devices, human factors/usability engineering focuses on the interactions between users, the use environment, and the device itself.
- The goal is to minimize use-related hazards and risks and then confirm that users can use the device safely and effectively.



- In May, 2015, the FDA convened the Gastroenterology-Urology Devices Panel of the Medical Devices Advisory Committee Meeting to seek expert scientific and clinical opinion related to reprocessing of duodenoscopes based on available scientific information.⁵⁴
- It is important to **consider the device, end user, and use environment** when developing reprocessing instructions.
- **Human Factors testing plays an important role in ensuring that end users will be able to understand and correctly follow the reprocessing instructions in the labeling.**
- Based on the panel's recommendation, the **FDA is considering the role of Human Factors testing in the development of reprocessing instructions as part of premarket assessment and review.**

Design Verification & Validation for Infection Prevention

Ex

Usability Study: Duodenoscope Reprocessing

- Q: How to ensure that user materials included in duodenoscope labeling and instructions for use are sufficient to ensure user adherence to reprocessing instructions?
- A: Put users into simulated-use studies and make sure they succeed in what the manufacturer intends for disinfection.
- Validation study participants should be representative of the professional staff that would perform these actual reprocessing procedures.



AER

- FDA has given guidance for sterilizing devices for over 30 years dating back to Blue Book Memorandum #G95-1.
- FDA recognizes various standards for sterilization validation:
 - ISO 11135 Ethylene Oxide
 - ISO 11137-1/2/3 Radiation
 - ISO 17665-1 Steam
- Practical aspects of sterilization validation:
 - Conducted after device and packaging design finalized
 - Often outsourced to specialized contract laboratory
 - Typically done along with related testing for bioburden and pyrogens

Conclusions

Ex

- Medical device infections lead to significant rates of patient morbidity & mortality, place an enormous cost burden on our health care system, and expose manufacturers to the risk of product liability litigation.
- These infections can be minimized by good design practices, including human factors and technologies that inhibit bacterial growth on implanted devices.
- Design verification & validation of infection prevention is necessary for single use devices (*i.e.*, sterilization validation) and reusable devices (*i.e.*, usability study of reprocessing).

Q & A

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Thank You!

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Contact

Howard M. Loree II, Ph.D.

Biomedical Engineering Manager

1075 Worcester St. | Natick, MA 01760

Office 508-903-4637 | Cell 617-780-6334

Email hloree@exponent.com | Website www.exponent.com

- At the request of Medmarc, Exponent accessed publicly available information regarding medical device infections and design approaches for prevention. The scope of services performed during this investigation may not adequately address the needs of all users, and any re-use of this report or its findings, conclusions, or recommendations presented herein are at the sole risk of the user.
- The opinions and comments formulated during this assessment are based on observations and information available at the time of the investigation. Exponent's role is advisory in nature and the opinions, analysis, conclusions, results, recommendations, and the like will be assessed by users with respect to their own products, processes, or services. As such, no guarantee or warranty as to the accuracy of this report is expressed or implied.
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